Localized Immunotherapy via Liposome-ANCHORED Anti-CD137 + IL-2 Prevents Lethal Toxicity and Elicits Local and Systemic Antitumor Immunity

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Abstract

Immunostimulatory agonists such as anti-CD137 and interleukin (IL)-2 have elicited potent antitumor immune responses in preclinical studies, but their clinical use is limited by inflammatory toxicities that result upon systemic administration. We hypothesized that by rigorously restricting the biodistribution of immunotherapeutic agents to a locally accessible lesion and draining lymph node(s), effective local and systemic antitumor immunity could be achieved in the absence of systemic toxicity. We anchored anti-CD137 and an engineered IL-2Fc fusion protein to the surfaces of PEGylated liposomes, whose physical size permitted dissemination in the tumor parenchyma and tumor-draining lymph nodes but blocked entry into the systemic circulation following intratumoral injection. In the B16F10 melanoma model, intratumoral liposome-coupled anti-CD137 + IL-2Fc therapy cured a majority of established primary tumors while avoiding the lethal inflammatory toxicities caused by equivalent intratumoral doses of soluble immunotherapy. Immunoliposome therapy induced protective antitumor memory and elicited systemic antitumor immunity that significantly inhibited the growth of simultaneously established distal tumors. Tumor inhibition was CD8+ T-cell–dependent and was associated with increased CD8+ T-cell infiltration in both treated and distal tumors, enhanced activation of tumor antigenspecific T cells in draining lymph nodes, and a reduction in regulatory T cells in treated tumors. These data suggest that local nanoparticle-anchored delivery of immuno-agonists represents a promising strategy to improve the therapeutic window and clinical applicability of highly potent but otherwise intolerable regimens of cancer immunotherapy.

Introduction

Immunostimulatory antibodies and cytokines elicit potent antitumor immunity in a variety of tumor models, often via the activation of cytotoxic T lymphocyte (CTL) and natural killer (NK) cell responses. Interleukin (IL)-2 stimulates the proliferation and effector functions of both CTLs and NK cells and has been approved for the treatment of advanced metastatic melanoma and renal cell carcinoma (1–3). Similarly, agonistic antibodies against the costimulatory receptor CD137 (4-1BB) expressed on the surface of activated T cells, NK cells, and dendritic cells potently inhibit tumor progression in preclinical mouse models and have begun testing in clinical trials (4–10). The priming of a CTL-mediated immune response is particularly attractive as it has the potential to target and eradicate recurrences or metastases in a tumor-specific manner (11–14). Nevertheless, the clinical use of immunomodulatory agonists has been hindered by dose-limiting inflammatory toxicities that often accompany systemic administration (15, 16). Intra-venous anti-CD137 elicits liver inflammatory damage, systemic inflammatory cytokine release, hematologic abnormalities, and disruptions in lymphocyte trafficking (4, 17, 18), whereas IL-2 therapy is accompanied by potentially lethal side effects such as capillary leak syndrome (19, 20). Although local injections may reduce the systemic exposure to potent immuno-agonists (21–24), such approaches remain inherently dose-limited, as soluble proteins rapidly reach the systemic circulation following intra- or peritumoral injection, via lymphatic drainage or direct entry into leaky tumor vasculature (25–30).

We recently developed a strategy to block systemic side effects from anti-CD40 and CpG oligonucleotides, 2 potent antitumor therapeutics, by locally administering these immuno-agonists conjugated to liposomal nanoparticles (25). Intratumorally (i.t.) injected anti-CD40/CpG liposomes dispersed throughout the tumor matrix and entered local lymphatics but were restricted from penetrating tumor vasculature or reaching the systemic circulation, thus prolonging the local immunotherapy exposure while eliminating...
symptoms of liver toxicity and systemic cytokine storms observed following soluble i.t. therapy. Although i.t. anti-CD40/CpG liposomes delayed the progression of established tumors in the poorly immunogenic B16F10 melanoma model (25), this treatment combination failed to induce complete/durable tumor rejections. We hypothesized that anti-CD137 and IL-2 co-delivered via this liposome-anchored approach would synergistically activate tumor-specific T lymphocytes in the tumor and tumor-draining lymph nodes (TDLN), thereby priming effective local immune responses and the systemic dissemination of CTLs capable of targeting distal untreated lesions (31, 32).

Using the murine B16F10 model, we show here that local therapy with anti-CD137 liposomes and IL-2 liposomes leads to potent antitumor activity with no evidence for systemic toxicity, unlike i.t. soluble anti-CD137 + IL-2 treatment. Importantly, control of local tumor progression by i.t. liposome therapy was accompanied by systemic antitumor immune responses, which restrained the growth of simultaneously established distant tumors. Thus, liposomal delivery enables aggressive local treatment with high doses of immunotherapeutic agents, promoting a systemic immune response without systemic toxicity.

Materials and Methods

Materials

Anti-CD137 (clone LOB12.3), anti-CD8a (clone 2.43), anti-NK1.1 (clone PK136), and rat IgG isotype control antibodies were from BioXCell. Dioleoylphosphocholine (DOPC), polyethylene glycol (PEG)2000-distearoylphosphoethanolamine (DSPE), maleimide-PEG2000-DSPE (Avanti Polar Lipids), and lipid tracer DiD (Invitrogen) were used as received. Fluorescent antibodies against mouse CD45, CD3, CD8a, CD4, NK1.1, Thy1.1, IFN-γ, and Foxp3 were from ebioscience. The Cytometric Bead Array Mouse Inflammation Kit was from BD Biosciences.

Preparation of anti-CD137 liposomes and IL-2Fc liposomes

IL-2Fc was prepared as a bivalent fusion of the N-terminus of anti-CD137 and IL-2Fc, respectively, coupled liposomes (lip-αCD137) and IL-2Fc-coupled liposomes (lip-IL-2Fc) were prepared as previously described (25): briefly, liposomes were first prepared with a composition of cholesterol/DOPC/PEG-DSPE/maleimide-PEG-DSPE at 35/60/2.5/2.5 or 35/62.5/0/2.5 mol% for Lip-αCD137 or Lip-IL-2Fc, respectively, and with 0.1 mol% of the fluorescent dye DiD for labeling. Anti-CD137 and IL-2Fc were treated with 1.8 mmol/L dithiothreitol to expose hinge region thiols and then mixed with liposomes for covalent maleimide-thiol conjugation. Conjugated liposomes were washed with PBS to remove unbound protein. The quantification of liposome-bound anti-CD137 or IL-2Fc was conducted by ELISA following solubilization of liposomes in 0.5% Tween-20 buffer. Endotoxin levels in Lip-αCD137 and Lip-IL-2Fc were found to be less than 1 EU/mg of liposomes by LAL assay (Pierce).

In vitro bioactivity of Lip-αCD137 and Lip-IL-2Fc

C57BL/6 splenocytes were polyclonally activated for 2 days, carboxyfluorescin succinimidyl ester (CFSE)-labeled, and then repleted with 20 ng/mL IL-2 (Peprotech). IL-2Fc, or Lip-IL-2Fc (equivalent molar doses). Specific binding of fluorescent IL-2Fc liposomes to T cells was assessed by flow cytometry after 2 hours, whereas total live cell counts and CFSE dilution were analyzed after 48 hours. In parallel, activated splenocytes were cultured with IL-2 for days 2 to 4, followed by 5 μg/mL soluble anti-CD137 or Lip-αCD137. Binding of fluorescent anti-CD137 liposomes was analyzed after 2 hours, and culture supernatants were collected after 24 hours for the measurement of IFN-γ by ELISA.

In vivo tumor therapy

Mice were handled in the USDA-inspected MIT Animal Facility following federal, state, and local guidelines. Six- to 8-week-old female C57BL/6 mice (Jackson Laboratory) were inoculated subcutaneously with 5 × 10^8 B16F10 cells (authenticated from American Type Culture Collection, cultured <6 months before use) on a single flank or both hind flanks. Tumor area was calculated as the product of 2 measured orthogonal diameters (D1 × D2). Mice were treated on one flank with intratumoral injections on days 9/12/16 unless otherwise indicated, using PBS, soluble anti-CD137 + IL-2Fc, Lip-αCD137 + Lip-IL-2Fc, or rat IgG isotype-liposomes (Lip-IgG), at an equivalence of 100 μg antibody + 20 μg IL-2 per dose unless otherwise indicated. For in vivo depletion, 400 μg/dose of anti-CD8a or anti-NK1.1 were injected intraperitoneally on days 7/12/16. To assess establishment of tumor-specific memory responses, single tumor-bearing mice were treated as described above, and at 4 or 8 weeks post-primary inoculation, a secondary challenge of 5 × 10^8 B16F10 cells was inoculated into the opposite hind flank and monitored without additional therapy. Weights of treated mice were measured daily as an indicator of body condition and systemic toxicity. Serum levels of anti-CD137 or IL-2 were quantified by ELISA, and serum cytokines were measured by Cytometric Bead Array (BD Biosciences). For additional tumor models, Balb/c mice (Jackson Laboratory) or C57BL/6 mice were inoculated s.c. on a single flank with 2 × 10^6 A20 cells (ATCC, cultured <6 months before use) or 3 × 10^5 TC-1 cells (authenticated and received from Dr. T.C. Wu, Johns Hopkins University, Baltimore, MD), respectively, then treated on days 7/9/11 postinoculation with intratumoral injections of PBS or Lip-αCD137 + Lip-IL-2Fc (75 μg antibody + 15 μg IL-2 per dose).

Flow cytometry and histological analysis

Mice with B16F10 tumors on both hind flanks were injected with DiD-labeled Lip-IgG, Lip-αCD137 + Lip-IL-2Fc, or saline on one flank only. The treated and contralateral tumors, proximal and contralateral TDLNs, and spleens were harvested and dissociated into single-cell suspensions for flow cytometry analysis on a FACSCanto II (BD Biosciences). Regulatory T-cell (Treg) levels were quantified by intracellular Foxp3 staining. For histologic analysis, treated tumors or TDLNs were snap-frozen for cryosection. Tissue...
sections were imaged on a Zeiss LSM 510 confocal microscope for the presence of DiD-labeled liposomes, with or without CD3/B220 co-staining. For pharmacokinetic analysis, treated tumors were harvested at indicated time points and digested in Tissue Protein Extraction Reagent + Halt Protease Inhibitor Cocktail (Pierce); supernatants from homogenized tissues were then analyzed by fluorescence for DiD concentrations and by ELISA for concentrations of anti-CD137 and IL-2Fc.

**Ex vivo T-cell activation**

IFN-γ production by lymphocytes was assessed by placing single-cell suspensions from TDLNs in culture for 12 hours, with or without phorbol 12-myristate 13-acetate (PMA; 50 ng/mL) + ionomycin (1 μmol/L) re-stimulation, followed by addition of brefeldin A for 5 hours. Intracellular IFN-γ was analyzed by flow cytometry, whereas *ex vivo* culture supernatants were analyzed by ELISA for secreted cytokine.

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**Figure 1.** Anti-CD137-liposomes (Lip-αCD137) and IL-2Fc-liposomes (Lip-IL-2Fc) are bioactive for T-cell binding and stimulation in vitro. A, schematic of immunoliposome preparation. B, flow cytometric histograms of activated CD4+ and CD8+ T cells after 2 hours of incubation in vitro with fluorescently labeled Lip-IL-2Fc or Lip-αCD137 (solid unfilled), unconjugated liposomes (dashed unfilled), or no liposomes (gray filled). C, *in vitro* T-cell proliferation after 48-hour incubation with Lip-IL-2Fc, IL-2Fc, or IL-2 as measured by cell counts (normalized to unstimulated cells) or CFSE dilution. **, P = 0.002; ****, P < 0.0001. D, IFN-γ production by polyclonal T cells stimulated by Lip-αCD137, isotype control liposomes, or soluble anti-CD137 after 24 hours. **, P = 0.0002; ***, P < 0.0001.
Adoptive transfer of B16 tumor-specific CD8+ T cells

Naïve CD8+ T cells expressing a transgenic T-cell receptor (TCR) specific for the B16 melanoma self-antigen gp100 (33) were isolated from female Thy1.1+ Pmel-1 mice (Jackson Laboratory) using a CD8 Negative Isolation Kit (Stemcell Technologies), CFSE-labeled, and then adoptively transferred (2 × 106 cells/mouse) into B16F10 tumor-bearing mice on day 7 posttumor inoculation. Mice were treated with i.t. liposome therapy as previously described, and the treated and contralateral TDLNs were excised on day 14 for flow cytometric analysis of CFSE dilution in CD8+ Thy1.1+ Pmel cells.

Statistical analysis

Data are shown as mean ± SEM. Average tumor growths were compared using 2-way ANOVA, and Kaplan–Meier survival curves were compared by log-rank test. For all other data, comparisons of 2 experimental groups were analyzed by 2-tailed unpaired t-tests. Statistical analysis was conducted using GraphPad Prism software.

Results

Liposome-anchored anti-CD137 and IL-2Fc retain potent bioactivity

We first prepared liposome-anchored immunotherapeutics by conjugation of monoclonal anti-CD137 or an engineered murine IL-2Fc fusion protein (Gai and Wittrup, manuscript in preparation) to the surfaces of PEGylated liposomes (Fig. 1A). Reduced disulfides of the Fc hinge region were linked to maleimide-terminated phospholipids on the liposomes, yielding 130 ± 10 μg of conjugated anti-CD137 or 53 ± 7 μg of conjugated IL-2 (cytokine equivalence) per mg liposomes. Anti-CD137–coupled liposomes (Lip-αCD137) and IL-2Fc–coupled liposomes (Lip-IL-2Fc) were then size-excluded by membrane filtration to a mean diameter of 160 ± 10 nm before use. Liposome-anchored IL-2Fc and αCD137 showed specific binding to activated murine CD4+ and CD8+ T cells in vitro (Fig. 1B) and retained T-cell stimulatory activity: CD4+ and CD8+ T cells showed similar levels of proliferation in response to equivalent doses of soluble IL-2, soluble IL-2Fc, or Lip-IL-2Fc (Fig. 1C), whereas Lip-αCD137 was ~6-fold more potent than soluble αCD137 in inducing IFN-γ secretion from activated T cells (Fig. 1D).

Intratumorally injected Lip-αCD137 + Lip-IL-2Fc therapy is locally retained and minimizes systemic exposure, preventing lethal systemic inflammatory toxicity

As anti-CD137 and IL-2 elicit significant inflammatory toxicity upon systemic administration (17–19), we examined whether nanoparticle anchoring would enable local retention of these agents without systemic dissemination following intratumoral injections, to minimize systemic toxicity. Subcutaneous B16F10 tumors were injected i.t. with fluorescently labeled Lip-αCD137 (100 μg antibody) and Lip-IL-2Fc (20 μg IL-2), on day 10 posttumor inoculation. Figure 2A shows representative histology 24 hours after injection, showing the presence of liposomes throughout the tumor. Fluorescence measurements from homogenized tumor tissues showed that liposomes persisted at the treated tumor for about 96 hours postinjection (Supplementary Fig. S1A), whereas anti-CD137 and IL-2 were detectable up to 48 hours after liposome injection (Supplementary Fig. S1B). Histologic sections of TDLNs taken at 24 hours postinjection showed liposome accumulation primarily in the subcapsular sinuses, consistent with direct lymphatic drainage (Fig. 2B and Supplementary Fig. S2).

In parallel, we measured serum levels of αCD137 and IL-2Fc 18 hours following a single i.t. dose of either liposome-coupled or soluble therapy. In contrast to soluble anti-CD137 + IL-2Fc, i.t. liposome therapy resulted in minimal detectable levels of either agonist in the blood (Fig. 2C and D), confirming the ability of immuno-liposomes to physically restrict these locally injected therapeutics. Flow cytometric analysis on day 14 following i.t. treatment of B16F10 tumors on days 9 and 12 showed that about 65% of tumor-infiltrating CD8+ T cells and NK cells were labeled with immunoliposomes, whereas isotype control liposomes (Lip-IgG) showed substantially lower nonspecific binding (Fig. 2E). Immunoliposomes also bound to 5% to 15% of CD8+ T cells in the proximal TDLNs but were not detectable in spleens or distal lymph nodes following intratumoral injections (Fig. 2F), confirming that lymphatic drainage of liposomes was confined to the treatment-proximal lymph node.

We next tested whether the dramatic reduction in systemic exposure achieved by liposome-anchored delivery impacted the systemic toxicity of αCD137 + IL-2Fc therapy. Soluble i.t. doses of αCD137 + IL-2Fc (days 9/12/16) induced significant elevations in serum levels of inflammatory cytokines (Fig. 3A) and rapid weight loss (Fig. 3B), accompanied by shivering, sluggish mobility, and other symptoms consistent with the measured systemic cytokine storm; these side effects were fatal in 2 of 8 soluble-treated animals (Fig. 3B). Mice treated with half-doses of soluble therapy (50 μg αCD137 + 10 μg IL-2Fc per dose) experienced comparable weight loss and fever-like symptoms, although without lethality (Fig. 3B). In contrast, full doses of i.t. Lip-αCD137 + Lip-IL-2Fc elicited only minimal increases in systemic cytokines compared with PBS-treated mice, at 1, 2, 3, or 5 days after the start of therapy (Fig. 3A and data not shown). Furthermore, i.t. liposome-treated mice did not exhibit weight loss or other physiologic symptoms of systemic cytokine release (Fig. 3B). Interestingly, intravenous administration of Lip-αCD137 + Lip-IL-2Fc induced intermediate systemic inflammation (Supplementary Fig. S3), indicating that liposome-mediated elimination of toxicity was dependent on the restricted biodistribution of liposomes at the treated tumor and TDLNs. Thus, local liposome treatment enabled the safe administration of an otherwise intolerable dose of this immunostimulatory therapy.

Intratumoral immunoliposome therapy regresses primary tumors and induces protective antitumor memory

To test the antitumor efficacy of immunoliposomes versus systemically disseminating soluble therapy, C57Bl/6 mice bearing s.c. B16F10 tumors were given i.t. injections of PBS, control Lip-IgG, Lip-αCD137 + Lip-IL-2Fc (100 μg αCD137 +
Figure 2. Anti-CD137 and IL-2Fc immunoliposomes are locally confined following intratumoral administration, minimizing systemic exposure. Established s.c. B16F10 tumors were injected i.t. with PBS, soluble anti-CD137 (100 μg) + IL-2Fc (20 μg IL-2) or equivalent doses of Lip-αCD137 + Lip-IL-2Fc. A and B, representative cryosections of a B16F10 tumor (dashed line indicates tumor boundary; A) and the TDLNs (B), 24 hours postinjection of fluorescently labeled immunoliposomes (white). Scale bars, 500 μm. C and D, serum levels of anti-CD137 (C) and IL-2Fc (D) were analyzed 18 hours postinjection. *, P < 0.0001; E, mice (n = 5–9) received 2 i.t. doses of control Lip-IgG or Lip-αCD137 + Lip-IL-2Fc on days 9 and 12 posttumor inoculation, and tumors were analyzed by flow cytometry on day 14 for the percentage of DiD⁺ (liposome-) cells among CTLs or NK cells. *, P = 0.0005; **, P < 0.0001. F. mice (n = 5–9) were treated i.t. as in E and the proximal TDLNs, contralateral LNs, and spleens were analyzed on day 14. *, P = 0.01.

To test whether Lip-αCD137 + Lip-IL-2Fc therapy established tumor-specific immunological memory, B16F10 tumor-bearing mice were treated as above and then challenged 27 days post-primary inoculation with a secondary challenge of 5 × 10⁴ B16F10 cells on the distal flank. All liposome-treated animals and 7 of 8 soluble-treated animals rejected the secondary challenge (irrespective of whether the primary tumor had been completely cured), whereas control naïve animals or mice bearing PBS-treated primary tumors all showed rapid tumor outgrowth (Fig. 4B). An additional distal tumor challenge on day 55, conducted on a subset of previously liposome-treated animals, was again completely rejected whereas untreated animals showed rapid tumor progression (data not shown).

Local immunoliposome therapy induces systemic antitumor immunity against untreated distal tumors

To determine whether localized immunoliposome therapy initiated a systemic antitumor immune response capable of targeting distal tumors, mice were inoculated with B16F10 cells s.c. on both hind flanks simultaneously and treated with
i.t. liposomes in one flank. Treated tumors were either completely cured (89%) or showed significantly delayed progression (Fig. 5A), whereas contralateral untreated tumors were also strongly inhibited (Fig. 5A and B), with 22% of dual tumor-bearing animals achieving rejection of the distal simultaneously established tumor (Fig. 5B). A prolonged treatment regimen did not further enhance the inhibition of distal untreated tumors, although i.t. treated tumors that had escaped the initial antitumor response could be arrested by extended therapy (Supplementary Fig. S6). Importantly, no symptoms of inflammatory toxicity were detected during the inflammatory toxicity window. Systemic (intraperitoneal) injections of low-dose soluble anti-CD137 (10 μg) + IL-2Fc (2 μg) showed no therapeutic effect against subcutaneous tumors (data not shown), suggesting that distal tumor inhibition following immunoliposome therapy was mediated by a disseminated immune response and not by low levels of immunotherapeutic agents leaking to the distal site.

We next assessed the relative importance of CD8+ T cells and NK cells in antitumor responses elicited by Lip-αCD137 + Lip-IL-2Fc. In the dual tumor B16F10 model, CD8+ depletion almost completely abrogated the efficacy of immunoliposome therapy (Fig. 6A), and the survival of liposome-treated CD8-depleted mice was not statistically different from untreated animals (Fig. 6B). In contrast, no loss in efficacy was detected in NK cell–depleted liposome-treated mice (Fig. 6A and B). Thus, although immunoliposomes bound to both CTLs and NK cells in treated tumors and tumor-proximal lymph nodes (Fig. 2E and F), only CTLs were required for protective immunity in this model.

Lip-αCD137 + Lip-IL-2Fc therapy induces an immunomodulated milieu at tumors and TDLNs

To evaluate immunologic changes in the tumor microenvironment following i.t. Lip-αCD137 + Lip-IL-2Fc therapy, we quantified the levels of tumor-infiltrating CTLs and regulatory T cells (Treg) in B16F10 dual tumor-bearing mice. In untreated or Lip-IgG–treated tumors, low levels of CTLs were detected at day 15, similar to pretreatment levels on day 9 (Fig. 7A), whereas CD4+ CD45+ Foxp3+ Treg became prevalent by day 15 (Fig. 7B), characteristic of an immunosuppressive tumor microenvironment (34–36). In contrast, we observed an approximately 21-fold increase in CTLs within immunoliposome–treated tumors by day 15 (Fig. 7A), as well as significantly
As immunoliposomes also access T cells in the TDLNs (Fig. 2B and F), we evaluated whether lymph node–resident T cells were primed following liposome therapy, by analyzing IFN-γ production in response to ex vivo re-stimulation. We found increased numbers of IFN-γ–producing CD8+ and CD4+ T cells in both treated and contralateral TDLNs of dual tumor-bearing mice on day 14 compared with untreated controls (Fig. 7D and E), showing an impact on immune responses in distal nodes despite the absence of direct liposome stimulation at those lymph nodes (Fig. 2F). Re-stimulated lymphocytes from

![Diagram of tumor growth curves](image_url)

**Figure 4.** Local immunoliposome therapy eliminates B16F10 tumors and elicits protective antitumor memory. A, individual tumor growth curves from mice inoculated s.c. with 5 × 10^6 B16F10 tumor cells, then treated i.t. on days 9/12/16 (arrows) with PBS, control Lip-IgG, Lip-αCD137 (100 μg) + Lip-IL-2Fc (20 μg IL-2), or the maximum tolerable dose of soluble anti-CD137 (50 μg) + IL-2Fc (10 μg IL-2). Boxed fractions indicate complete rejections of the tumors. B, primary tumors were treated as described for A, followed by a secondary inoculation of 5 × 10^6 B16F10 cells s.c. in the opposite flank on day 18 for PBS-treated mice or on day 27 for immunoliposome-treated and soluble-treated mice. Naïve animals without primary tumors were simultaneously inoculated to validate tumor cell viability. Boxed fractions indicate complete rejections of the secondary tumor challenge.

increased levels of CTLs in the contralateral tumors (Fig. 7A), despite the absence of detectable liposomes in the distal tumor (data not shown). T<sub>reg</sub> accumulation was also blocked in tumors treated with i.t. Lip-αCD137 + Lip-IL-2Fc, although not in the contralateral tumors of these mice (Fig. 7B). Calculated CTL/T<sub>reg</sub> ratios thus showed a substantial shift in immune activation within both treated and contralateral tumors in liposome-treated mice compared with untreated controls (Fig. 7C). NK cell levels were unaffected in treated or contralateral tumors following immunoliposome therapy (Supplementary Fig. S7), consistent with the lack of impact of NK cell depletion.

**Figure 5.** Local immunoliposome therapy elicits systemic immunity that inhibits simultaneously established distal tumors. Mice (n = 9–10) were inoculated s.c. with B16F10 tumors on both hind flanks simultaneously, then treated i.t. on one flank with PBS or Lip-αCD137 + Lip-IL-2Fc on days 9/12/16 (arrows). A, average growths of treated tumors and contralateral untreated tumors. *P = 0.002; **P = 0.009; ***P < 0.0001. B, individual growth curves of contralateral untreated tumors in i.t. PBS-treated or immunoliposome-treated mice. Boxed numbers indicate fraction of long-term cures.

![Diagram of tumor growth curves](image_url)
the proximal draining lymph nodes of liposome-treated mice also secreted about 5-fold more IFN-γ than lymphocytes from untreated mice, signifying greater per-cell secretion in addition to the increased frequency of IFN-γ–producing cells (Fig. 7F).

To gain further insight into how i.t. immunoliposome therapy mediated a systemic antitumor response, we examined the de novo priming of tumor-specific T cells in TDLNs. CFSE-labeled, naïve Pmel-1 CD8+ T cells, which express a transgenic TCR specific for the B16 self-antigen gp100 (32), were adoptively transferred into dual tumor-bearing mice before immunoliposome therapy in one tumor only. At day 14, a basal level of Pmel proliferation was observed in the lymph nodes of untreated tumor-bearing mice (Fig. 7G and H). However, Pmel cells recovered from the treatment-proximal and contralateral lymph nodes of immunoliposome-treated mice trended toward a greater number of divisions (Fig. 7G and H), consistent with the therapeutic activation of endogenous lymph node–resident CTLs described above (Fig. 7D–F). The range of proliferative responses observed at the treatment-proximal lymph nodes may reflect the variability in tumor burden reduction at this time point. Interestingly, transferred Pmel cells were not detected on day 14 in either treated or contralateral tumors, nor in control untreated tumors (data not shown), indicating that tumor-specific CTLs activated at the lymph nodes of liposome-treated mice had not yet trafficked to tumor lesions. This suggests that the early inhibition of distal tumor growth was mediated by the dissemination of stimulated CTLs originating from the treated tumor.

**Discussion**

Previous studies have established the antitumor efficacy of anti-CD137 and IL-2, particularly as a combination therapy (31, 37–42). However, significant inflammatory toxicities have been observed in preclinical and clinical studies of both agents (4, 8, 17–19), limiting the dosages that can be tolerated in patients. Here we show that liposome conjugation enables intratumoral administration of a highly efficacious regimen of anti-CD137 + IL-2 therapy in the complete absence of the severe systemic toxicities elicited by systemic or local administration of equivalent soluble doses. In addition to complete regression of a majority of locally treated tumors, Lip-αCD137 + Lip-IL-2Fc primed systemic immunity that inhibited established distal tumors and rejected secondary tumor inoculations after the cessation of therapy. The increased frequency of CTLs within both treated and distal untreated tumors following Lip-αCD137 + Lip-IL-2Fc therapy, the loss of efficacy in CD8-depleted mice, and the increased number of activated IFN-γ–producing CTLs in proximal and contralateral TDLNs all provided evidence for combined local and systemic CTL-mediated antitumor immunity.

Preclinical studies of intratumorally administered soluble immunotherapies have shown reduced systemic side effects by decreasing the dosages required for tumor inhibition while eliciting both local and systemic tumor regression (11, 12, 21, 22, 43). Similar findings were recently reported by Levy and colleagues in a phase I/II study of local CpG injection.
were calculated (H). CFSE dilution in Pmel-1 cells from TDLNs was analyzed on day 14 by flow cytometry to determine numbers of tumor-infiltrating CTLs (A, **P < 0.01; ***P < 0.001). On day 14, cells from treatment-proximal and contralateral TDLNs were cultured ex vivo for 12 hours with or without PMA/ionomycin restimulation and IFN-γ-producing CD8⁺ (D) and CD4⁺ (E) T cells were enumerated by intracellular cytokine staining. *, P < 0.05; **, P < 0.01; ***P < 0.001. F, culture supernatants were analyzed by ELISA for secreted IFN-γ, ***, P < 0.001. G and H, dual tumor-bearing mice received an adoptive transfer of 2 × 10⁶ native CFSE-labeled Pmel-1 cells on day 7; then were treated on days 9 + 12 as above. CFSE dilution in Pmel-1 cells from TDLNs was analyzed on day 14 by flow cytometry (G), and mean division indices (mean divisions per cell) were calculated (H). **, P < 0.01; N.S., not significant.

Combined with local radiation therapy (23, 44). In addition, Fransen and colleagues (22) showed that low doses of anti-CD40 can be locally injected without toxicity by formulation in a slow-release emulsion, although a 5-fold higher dose administered via the same formulation was reported to cause liver inflammation. This finding highlights the fact that locally administered soluble antibodies or cytokines remain capable of leaking into systemic circulation, even if delivered via controlled release vehicles, depending on the dosage administered (22, 26–30, 45). In contrast, the nanoparticle-anchoring strategy described here physically restricts immuno-agonists at the local injection site even when administered repeatedly at
high doses while retaining efficacious local and systemic antitumor immunity.

Combined Lip-ocCD137 + Lip-IL-2Fc therapy exhibited much greater efficacy than monotherapy with either agent alone. Preliminary data from our laboratory have shown that i.t. IL-2 therapy induces the upregulation of CD137 receptor expression on tumor-infiltrating CD8+ T-cells (B. Kwong and D.J. Irvine, unpublished observations), analogous to observations by Redmond and colleagues (40) describing IL-2R-regulated increases in OX40 expression on CTLs. Palazon and colleagues (21) also recently showed that hypoxia blocks CD137 expression in tumor-infiltrating T cells, allowing intratumoral ocCD17 therapy to mediate local and distal tumor inhibition. Paradoxically, CD137 agonists alone or in combination with IL-2 have been shown to stimulate Treg cell expansion in vivo and in vitro (5, 46, 47), indicating a potential role in treating autoimmune conditions. Although we confirmed that combined Lip-ocCD137 + Lip-IL-2Fc induced moderate proliferation of sorted CD4+CD25–Foxp3– Treg in vitro (data not shown), i.t. Lip-ocCD137 + Lip-IL-2Fc therapy clearly blocked Treg accumulation within treated tumors and significantly enhanced tumor-infiltrating CTL:Treg ratios, a measure known to correlate with favorable antitumor immunity (48). Furthermore, immunoliposome therapy stimulated IFN-γ production in CD4+ T cells as well as CD8+ T cells in the proximal TDLNs, indicating the activation of effector CD4+ T cells.

Following liposome therapy, the growth of distal untreated tumors was significantly inhibited, correlating with an increased density of tumor-infiltrating CTLs. The absence of liposome accumulation at distal tumors and lymph nodes, the negligible levels of systemic inflammatory cytokines/chemokines following immunoliposome therapy, and the lack of Pmel T-cell infiltration into tumors after 1 week together suggested that these increased CTL levels did not result from de novo naïve T-cell priming at the TDLNs. Rather, immunoliposome therapy may have re-activated existing effector T cells in the i.t. treated tumor/TDLNs, which rapidly disseminated systemically to enact distal tumor inhibition, a phenomenon previously described by Straten and colleagues (49). This model remains consistent with the lack of detectable liposomes in the contralateral tumor if the disseminated T cells were indirectly stimulated in the i.t. treated site (and thus not directly labeled) or if liposomes were degraded during lymphocyte trafficking.

In conclusion, nanoparticle-mediated "anchoring" of immunotherapy biologics is a versatile strategy for priming antitumor immunity. By localizing the biodistribution of therapy, highly potent but previously intolerable immunotherapeutic regimens can be administered at large doses within an accessible lesion for the induction of systemic antitumor immunity without detectable systemic inflammation. In addition, this approach may be synergistic in combination with the administration of better-tolerated immunotherapy agents such as anti-CTLA-4 or anti-PD-1 that are known to promote tumor regression in humans (50).

Disclosure of Potential Conflicts of Interest
No potential conflicts of interest were disclosed.

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Conception and design: B. Kwong, D.J. Irvine
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Administrative, technical, or material support (i.e., reporting or organizing data, constructing databases): D.J. Irvine
Study supervision: D.J. Irvine

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